Radiological, biomechanical and histopathological characteristics of rat brain in Kaolin-induced hydrocephalus

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ABSTRACT

Objective: A better understanding of the pathophysiology and underlying mechanisms of brain damage in hydrocephalus is vital in developing diagnostic, observational and treatment tools that will have an impact on hydrocephalus outcomes. In this study, we aimed to demonstrate the radiological, biomechanical and histopathological characteristics of rat brain tissue in an experimental hydrocephalus model.

Materials and Methods: Thirty-six male Sprague-Dawley rats (21 days old, weighing between 150 and 200 grams) were used in this study. Animals were randomly assigned to control (n = 6), 1-week hydrocephalus (n = 10), 2-week hydrocephalus (n = 10) and 3-week hydrocephalus (n = 10) groups. Hydrocephalus was induced with cisternal kaolin injection and controls received sham injection. Magnetic resonance imaging was used to measure ventricle size and cortical thickness. Vital signs, cerebral blood flow (CBF), mechanical tests and brain histology were assessed.

Results: Three rats in the hydrocephalus group died during the follow-up, yielding an overall mortality of 10% among animals from hydrocephalus groups. Ventricular width, cross-sectional area of the lateral ventricles, ventricular index and ventricle / brain area ratio progressively increased and cortical thickness progressively decreased following kaolin injection. CBF was significantly lower at baseline than at 1st, 2nd and 3rd week (p < 0.05, for all). ICP was significantly elevated in all hydrocephalic groups in comparison with controls. EIT that was calculated from the first load-unload indentation test showed a significant increase at 2nd week post-injection (p=0.0001), indicating increased intracranial stiffness. However, this significant difference disappeared at 3rd week (p=0.956). Quantitative immunohistochemistry showed that hydrocephalic brains demonstrated significantly less NeuN-positive cells and significantly higher IBA-1-positive microglia and glial fibrillary acidic protein positive astrocytes cells in the cortex.

Discussion and Conclusion: Cisternal kaolin injection causes varying degrees of
ventricular enlargement in a rat model and hydrocephalus might contribute to neuronal and axonal damage and alter brain stiffness through axonal stretching or local hypoperfusion progressively over a period of days to months. As shown in this study, irreversible changes in viscoelastic behaviour and cellular structure develop in the late stages of hydrocephalus, suggesting the importance of early intervention in the treatment of hydrocephalus.

**INTRODUCTION**

The basic definition of hydrocephalus is “an abnormal accumulation of cerebrospinal fluid (CSF) within the ventricles of the brain” [13]. The estimated prevalence is 1–1.5% and the incidence of congenital hydrocephalus is approximately 0.9–1.8/1000 births [17,23]. Early onset hydrocephalus often results in the poorest neurological outcomes, with approximately 80% of patients suffering with residual neurological deficits [21].

Experimental animal models have been developed using various methods and agents to induce hydrocephalus or through genetic mutations in rodents. Although none of these models can fully mimic human condition, they can provide basic information that contributes to better understanding the pathogenesis of hydrocephalus and underlying causes. Although ventriculomegaly occurs naturally in congenital rat models, they are not ideal for long-term studies unless hydrocephalus is surgically intervened. Thus, the most common method of inducing experimental hydrocephalus without genetic mutation is the cisternal kaolin injection model that was introduced in the 1930s [19]. Kaolin is injected into the cisterna magna and spreads in the subarachnoid space, where it induces an inflammatory reaction and leads to an obstruction in the CSF pathways [8]. It is a simple, inexpensive and consistent way of inducing hydrocephalus in experimental animals [15].

Both clinical hydrocephalus and experimental hydrocephalus are often associated with symptoms of increased intracranial pressure (ICP) with ventricular dilatation. Understanding the biomechanical properties of the hydrocephalic brain can help in predicting mechanisms, simulating the disease and creating a treatment protocol. However, due to the complexity of the brain and the surrounding structures, data on the mechanical properties of living neural tissue is limited and variable [10,22].

In this study, it was aimed to demonstrate the radiological, biomechanical and histopathological features of rat brain tissue in kaolin-induced hydrocephalus model.

**MATERIALS AND METHODS**

All animal experiments were conducted in accordance with the Institutional Animal Care and Use Committee of Istanbul University guide for the care and use of laboratory animals in consultation with institutional veterinarians. Specific protocols used in this study were approved by Istanbul University Laboratory Animals Local Ethics Committee (2013/47). Anaesthesia, preoperative animal preparation, anaesthesia delivery, perioperative analgesia practices, and surgical protocols were optimized to minimize trauma to the animals.

Thirty-six male pathogen-free Sprague-Dawley rats (age, 21 days; weight, 150-200 g) were maintained on a 12-hour light/dark cycle and had free access to water and pellet food. Animals were randomly assigned to control group (n=6), one-week hydrocephalus group (n=10), two-week hydrocephalus group (n=10) and three-week hydrocephalus group (n=10). All hydrocephalus groups underwent cisternal 0.02 mL sterile kaolin (200 mg / mL kaolin in 0.9% saline solution) injections, whereas controls received sham injection. All groups underwent magnetic resonance imaging (MRI), mechanical tests and histopathological examination.

**Induction of Experimental Hydrocephalus**

Rats were anesthetized with ketamine HCl (Ketalar, Parke Davis-Eczaci大巴, Istanbul) and Xylazine (Rompun, Bayer, Istanbul) before surgical procedures. The head was secured in a stereotactic frame and a small vertical incision was made over the back of the neck from the top of the occiput to C1. The nuchal muscle layers were divided in the midline and retracted laterally to expose the atlanto-occipital membrane (FIGURE 1). In all rats in the hydrocephalus groups, 0.02 ml kaolin suspension was injected slowly into the cisterna magna through a 27-gauge needle. Control rats were subjected to sterile saline injection. The muscle layers and skin were sutured and rats were allowed to recover. After recovery from anaesthesia, rats were kept at room temperature and provided with standard chow and water ad libitum. They were examined daily for clinical signs of illness. Rats were weighed daily and monitored for neurological deficits.
FIGURE 1. Basic demonstration of animal preparation. Custom custom-made stereotactic frame (upper left), atlanto-occipital membrane (upper right), preparation of cranial windows (lower left), and cerebral blood flow measurement with laser speckle microcirculation imager and pressure transmitter probe in the cisterna magna for monitoring intracranial pressure (lower right) can be seen.
Magnetic Resonance Imaging

MRI studies were performed under general anaesthesia by the use of a human MR scanner equipped with a 48-cm bore magnet operating at a field of 1.5 T (Brivo MR355, GE Healthcare, Waukesha, US) with a custom coil to obtain T2-weighted images of the brain in the coronal plane. The total area of the lateral ventricles and the brain area were evaluated by a radiologist using the PACS workstation (Neorad®, Teleradiology & 3D, Serman Medical Information, Istanbul, Turkey) on the coronal brain section that includes the anterior wall of the third ventricle. The frontal ventricle-to-brain area ratio, ventricle width index and cortical thickness measurements were performed as described by Shulyakov et al. [26].

Animal Preparation

After MRI, spontaneously breathing rats were induced with 4% isoflurane gas delivered by 100% oxygen. The rats were placed in the supine position on a homoeothermic blanket system and instrumented with a rectal temperature probe and foot pulse oximeter to continuously monitor body temperature, blood oxygen saturation, and heart rate. Under the operating microscope, the trachea was intubated with a 16G tube through a tracheostomy. The rats were then maintained with mechanical ventilation at fixed tidal volume (7 mL/kg) and inspired oxygen (40%). The left common carotid artery was dissected and cannulated for continuous blood pressure monitoring, serial blood gas analysis and fluid replacement. Isoflurane was titrated to maintain a mean arterial pressure of 80-120 mm Hg and oxygen saturation >90%. The rats were then positioned prone, fixed in a custom-made stereotactic frame and previous midline incision was used to expose the skull. The periosteum was incised and dissected. The skull was bilaterally thinned using a high-speed drill equipped with a 1.8-mm diamond burr bit to create bilateral penetrating cranial windows, leaving the dura-arachnoid membranes intact. A pressure transmitter probe was inserted into the cisterna magna for monitoring ICP. For cerebral blood flow (CBF) measurement, Laser Speckle Microcirculation Imager was positioned over the rat with the desired cranial window aligned in the camera field of view. Speckle images within a 1.2-cm x 1.6-cm region were acquired at a frequency of 50 Hz with a resolution of 100 mm/pixel, with 18,526K points/perfusion unit value. Baseline images were recorded and CBF in arbitrary perfusion units was obtained throughout the procedure. Physiological data were recorded continuously during the procedure. Baseline and hourly blood gas levels were analysed in all animals. The core temperature was measured via rectal probes and used as a reference for brain temperature.

Mechanical tests

A custom-made indentation instrument with a half-spherical indenter was used. The indenter was fastened to the custom-made stereotactic frame and it was positioned over the centre of craniectomy to achieve a planar initial contact. With the use of previously described mechanical force parameters [27,31], a standard sequence of indentation tests including loading-unloading test, load and hold test, and multicycle loading-unloading test was performed. Indentation modulus (EIT), viscous deformation and viscous nature of the material were assessed. Recovery periods of approximately 15 minutes were allowed between tests.

Histological Examination

Animals were overdosed with pentobarbital after mechanical testing, and transcardially perfused with saline and then 4% paraformaldehyde. Brains were post-fixed and subsequently immersed in the same fixative solution overnight at 4 °C and then washed in phosphate-buffered saline and stored in ethanol until processing. Coronal slices were sectioned and embedded in paraffin. The paraffinized tissue slices were sectioned at 5 mm thickness. To assess neuronal integrity, activated microglia, and activated astrocytes, the following primary antibodies were used: anti-FOX3 (NeuN) 1:2000, anti-Iba-1 1:1000, and anti-glial fibrillary acidic protein (GFAP) 1:500. Images from the cortex were taken at 200x magnification. Using Image J, NeuN, Iba-1, and GFAP stained cells were counted.

Statistical analysis

Statistical analysis was performed using SPSS 18 (IBM Corp., Armonk, NY, USA). All data are expressed as mean ± standard error of the mean. Comparison across the groups was made by using analysis of variance. Statistical significance was accepted at p < 0.05.
RESULTS
In total, thirty rats underwent induction of hydrocephalus. None of the rats in the hydrocephalus groups experienced major neurological deficits. Three rats in the 3-week hydrocephalus group died during the study, yielding an overall mortality of 10% among animals from hydrocephalus groups. Two rats died during the 3rd week of hydrocephalus and no cause could be identified. One rat died during indentation testing, probably due to anesthesia overdose. Therefore, the assessments were performed with a total of 33 rats.

During the study, all animals, regardless of group, showed an increase in body weight (p < 0.0001). Hydrocephalic rats lost weight after kaolin injection, typically for 2–3 days. By 1-week post-injection, the rats started gaining weight. Nonetheless, rats in the hydrocephalus groups weighed less than controls regardless of hydrocephalus week (p=0.0014 for one-week hydrocephalus; p<0.0001 for two-week hydrocephalus and p<0.0001 for three-week hydrocephalus).

MRI imaging showed that the ventricular width, cross-sectional area of the lateral ventricles, ventricular index and ventricle / brain area ratio progressively increased and cortical thickness progressively decreased following kaolin injection (TABLE 1) (FIGURE 2).

<table>
<thead>
<tr>
<th></th>
<th>MRI parameters</th>
<th>Ventricular width</th>
<th>Cross-sectional area of the lateral ventricles</th>
<th>Ventricular index</th>
<th>Ventricle / brain area ratio</th>
<th>Cortical thickness</th>
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<tbody>
<tr>
<td><strong>Hydrocephalic rats</strong></td>
<td>1st week vs. 2nd week</td>
<td>&lt;0.0001</td>
<td>&lt;0.0001</td>
<td>&lt;0.0001</td>
<td>0.0005</td>
<td>0.0142</td>
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<td>&lt;0.0001</td>
<td>&lt;0.0001</td>
<td>&lt;0.0001</td>
<td>&lt;0.0001</td>
<td>&lt;0.0001</td>
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<td><strong>Control rats</strong></td>
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<td>0.99</td>
<td>0.96</td>
<td>0.86</td>
<td>0.87</td>
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<td></td>
<td>1st week vs. 3rd week</td>
<td>0.79</td>
<td>0.72</td>
<td>0.68</td>
<td>0.61</td>
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TABLE 1. Statistical evaluation of MRI parameters in hydrocephalic and control rats.

In control rats, CBF was significantly lower at baseline than at 1st, 2nd and 3rd week (p < 0.05, for all). Hydrocephalic rats also showed an increase in CBF with time, but this was not significant (p=0.2429). Hydrocephalic rats at 1st week had a lower CBF than controls; however, the difference was not significant.

FIGURE 2. Magnetic resonance image demonstrating increase in ventricular size in a hydrocephalic rat at 3rd week (right) compared to a control rat (left).
Characteristics of rat brain in Kaolin-induced hydrocephalus (p=0.3134). At 2nd and 3rd weeks, hydrocephalic rats had a significantly lower CBF than controls with a highest percentage reduction of 59% (p<0.0001) (TABLE 2).

<table>
<thead>
<tr>
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<th>Mechanical parameters</th>
<th>CBF</th>
<th>ICP</th>
<th>Heart rate</th>
<th>EIT</th>
<th>Strain during load-hold</th>
<th>Strain during multi-cycle</th>
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<td><strong>Hydrocephalic rats</strong></td>
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<td>0.1865</td>
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<td>0.0145</td>
<td>0.9443</td>
<td>&lt;0.0001</td>
<td>0.1340</td>
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<td><strong>Control rats vs. Hydrocephalic rats</strong></td>
<td>Control vs. 1st week</td>
<td>0.0004</td>
<td>&lt;0.0001</td>
<td>&lt;0.0001</td>
<td>0.8842</td>
<td>0.0002</td>
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<td>Control vs. 3rd week</td>
<td>&lt;0.0001</td>
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<td>&lt;0.0001</td>
<td>0.956</td>
<td>&lt;0.0001</td>
<td>0.0082</td>
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TABLE 2. Statistical evaluation of physiological and mechanical parameters in hydrocephalic and control rats
CBF: cerebral blood flow; ICP: intracranial pressure; EIT: indentation modulus

**Figure 3.** Representative histomicrographs showing significantly decreased NeuN-positive cells in the cortex of rats in the hydrocephalus group at 3rd week (b) compared to controls (a), and significantly increased Iba-1-positive microglia (red) and GFAP-positive astrocyte cells (gray) in the cortex of rats in the hydrocephalus group at 3rd week (d) compared to controls (c).
For the control and hydrocephalic groups, the indentation tests were associated with an ICP increase up to 20%. EIT that was calculated from the first load-unload indentation test showed a significant increase at 2nd week post-injection (148 kPa vs. 278 kPa, p=0.0001), indicating increased intracranial stiffness. However, this significant difference disappeared at 3rd week (p=0.956). In the load-hold indentation test, control and hydrocephalic brains exhibited gradual deformation and the associated intracranial strain was significantly greater at each time points in the hydrocephalus groups (p=0.0002 at 1st week, p=0.0001 at 2nd week and p<0.0001 at 3rd week). The multi-cycle indentation test also caused gradual deformation of the intracranial contents in all groups, but there was no significant difference between groups (p=0.0555 at 1st week, p=0.082 at 2nd week and p=0.176 at 3rd week) (TABLE 2).

Systemic blood pressure and mean arterial pressure were stable during mechanical tests; however, due to increased ICP, cerebral perfusion pressure and CBF decreased. After withdrawal of the indenter, blood flow returned immediately to baseline values in all groups. Baseline core temperatures were not statistically different between all groups and changes were not significant during indentation (TABLE 2).

ICP in controls was 6.5 ± 0.86 mmHg. Compared to controls, ICP was significantly elevated in all hydrocephalic groups, with the pressure being highest at 2nd week (p<0.0001 at all-time points). ICP showed a rapid pressure rise during indentation and returned immediately to baseline values after withdrawal in all groups. During indentation, bradycardia was identified at the point of maximal ICP (TABLE 2).

Quantitative analyses of NeuN-positive, IBA-1-positive, and GFAP-positive cells in the cortex of animals with hydrocephalus demonstrated significantly less NeuN-positive cells that reflects altered neuronal integrity, and significantly more Iba-1-positive microglia and GFAP-positive astrocyte cells that indicate higher inflammatory signals (FIGURE 3).

**DISCUSSION**

To investigate the radiological, biomechanical and histopathological changes in experimental hydrocephalus, we analyzed the impact of kaolin-induced hydrocephalus in rats. The present data indicate that kaolin-induced hydrocephalus created a reproducible hydrocephalus model with altered brain morphology along with disturbed mechanical properties and neuronal integrity.

Besides genetic mutations, experimental animal models have been developed using numerous agents to induce hydrocephalus [8,15]. All of these models provide important information to understand the causes and potential treatments of hydrocephalus. The most commonly used method is the injection of kaolin into the cisterna magna [9] and it is an inexpensive, simple and reliable method that has been previously studied in rats [6,7,11,12,18]. In our study, the experimental rats were particularly 21-day old rats, as it corresponds to the first 6-month period of human brain development in which cerebral myelination is rapid [24,30]. The rats in our study tolerated the kaolin injection fairly well with acceptable levels of mortality (10% died during 3 weeks, one possibly due to anesthesia overdose) and no evidence of hemorrhage was observed following removal of the brain. Compared to higher rates of mortality in the literature, it was thought that the difference might be due to post-operative animal care, animal breed used and the chemical properties of kaolin [5,20]. However, it should be noted that none of these models, including kaolin-induction method, is perfect in imitating human conditions.

Although kaolin-induced hydrocephalus model offers dose-dependent responses to some extent, there is variable dispersion of kaolin in the subarachnoid space, and this may account for the relatively unpredictable rate and magnitude of ventricular dilatation [8]. Consistent with the literature, in our study, kaolin presumably caused a moderate to severe hydrocephalus with a ventricle/brain area ratio of 0.105 ± 0.02 at 3 weeks, compared to 0.018 ± 0.002 at baseline. Kaolin causes an inflammatory response, thus causing blockage of the fourth ventricle and mimicking hydrocephalus caused by meningitis. Although this model has been criticized for its inflammatory effects such as evident macrophages, CD4- and CD8- lymphocytes in the subarachnoid space and in surrounding brain parenchyma, and reactive microglia in the white matter surrounding the ventricles [7,16,25], it was reported that kaolin had clearly been ingested by macrophages and there were minimal neutrophils and eosinophils at 10th day post-injection with histologically unaltered brainstem and cerebellum...
adjacent to kaolin collections [29]. Brain injury in hydrocephalus is a multifactorial process marked by ventricular enlargement leading to stretching of axons with concomitant cortical compression. However, these histologically evident progressive destructive changes can be difficult to quantify due to profound tissue distortions [16]. In our study, quantitative analyses of NeuN-positive, IBA-1-positive, and GFAP-positive cells in the cortex of animals with hydrocephalus demonstrated significantly less NeuN-positive cells and significantly more Iba-1-positive microglia and GFAP-positive astrocyte cells.

Due to the complexity of the brain and the surrounding meningeal structure, information about the mechanical properties of living neural tissue is insufficient [10, 22]. To learn about the mechanical changes and to better understand the physical mechanisms involved in hydrocephalus, it is necessary to learn about the mechanical properties of the brain in vivo [1]. The main advantage of in vivo testing is that the tissue structure remains largely intact, as close to its natural state as possible [4]. It is widely known that the mechanical properties of neural tissues are associated with their microstructure [2]. Thus, changes in tissue microstructure can be reflected as an altered stiffness. In our study, the live brain mechanical properties reflected a combination of several different anatomical and physiological systems including the dura mater, the intact CSF system, and the brain itself. The stiffness of cortical gray matter increased despite the differences in tissue microstructure at 2nd week, similar to the study by Shulyakov et al. [26]. However, Juge et al. [14] did not find such an increase in the same hydrocephalus rat model. The main difference of their study was that they used MR elastography to measure brain stiffness and the contribution of hydrostatic pressure to mechanical properties was eliminated by elastography analysis method [28]. Despite the increase at 2nd week, the difference between controls and hydrocephalic group disappeared at 3rd week. Regarding this, it can be suggested that microstructural rearrangement occurs in brain during chronic phase of hydrocephalus possibly through neuronal damage. This damage was also demonstrated in our study by significantly less NeuN-positive cells in the hydrocephalic group at 3rd week. The absence of permanent change in viscoelastic behaviour in the brain in the early stages of hydrocephalus in our study shows the importance of early intervention in the treatment of hydrocephalus.

The main limitation of our study was that we could not use an animal MRI equipped with a higher magnetic field strength. However, in a previous study, 1.0T MRI was shown to be a reliable equipment to assess MRI features in experimental hydrocephalus [3].

CONCLUSION
Cisternal kaolin injection causes varying degrees of ventricular enlargement in a rat model and reflects the hydrocephalus pathology seen in foetuses and premature infants in some aspects. Hydrocephalus might contribute to neuronal and axonal damage and alter brain stiffness through axonal stretching or local hypoperfusion progressively over a period of days to months. The absence of permanent change in viscoelastic behaviour in the brain in the early stages of hydrocephalus necessitates early intervention.

References


